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# Present and Future Trends in TiO<sub>2</sub> Nanotubes Elaboration, Characterization and Potential Applications

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*The paper is focused on TiO<sub>2</sub> nanotubes elaboration, characterization and potential applications, starting from the idea that monitoring anodizing conditions is a way to obtain nanotubes with various dimensions and various potential applications related to the change of hydrophilic – hydrophobic balance, biocompatibility, nano-porosity, stability, etc. Such properties are important for the use of Ti as biomaterial, as self-cleaning, solar energy conversion, controllable wettability, photocatalysis, etc. The electrochemical behaviour of the nanotubes was monitored by Tafel plots and open circuit potential determinations, and was discussed in connection with surface features evaluated from scanning electron microscopy, atomic force microscopy and contact angle measurements.*

**Keywords** Electrochemical stability; surface analysis; titania nanotubes

## 1. Introduction

It is well known that titanium and its alloys with a thin passive stratum, predominant TiO<sub>2</sub> represent materials providing excellent physical mechanical and biocompatible properties [1]. In the past, many attempts have been made to improve the surface properties of Ti-based materials by modifying topography, chemistry, and surface energy to better stability, or integrate into bone as implant materials. Such surface modification techniques included chemical methods as acid etching, and the use of various coatings) [2–5]. Through these approaches, a better performance in electrochemical stability and biocompatibility of Ti and Ti alloy has been achieved due to the creation of optimal micro-scale surface features.

In the last decade various groups of research begun exploring the formation of nanostructured materials, particularly the nanotopography of surfaces using self-organization. Different methods of self organization have been investigated as physical vapor deposition (PVD), MOCVD meniscus ordering of micro and nano-beads, and thin polymer films [6].

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Using all of these methods coatings with well-defined nanoscale surface properties were obtained and new applications were proposed [7,8]. In this approach, various techniques were performed in order to get  $\text{TiO}_2$  nanostructure and anodizing was a choice for a chip and convenient one. Changing anodizing parameters as voltage, pH electrolyte compositions and time of electrolysis a large variety of structure with various potential applications could be identify [9,10]. Such potential applications are related to the change of hydrophilic – hydrophobic balance, biocompatibility, nano-porosity, stability, properties important first for the use of Ti and Ti alloys as biomaterials, and in other fields, as self –cleaning, solar energy conversion, controllable wettability, electrochromic devices, photocatalysis, as well [8,9]. Anatase  $\text{TiO}_2$  nanocrystallites are considered to be the most active crystalline structure of  $\text{TiO}_2$  photocatalyst. Ultrafine anatase nanocrystallites, particles, less than 10 nm possess unique photochemical properties due to quantum size effects. It has been reported that Q-sized  $\text{TiO}_2$  nanocrystallites can expedite the diffusion of electrons and holes to the surfaces and inhibit electron-hole recombination through charge carrier trapping and, as a result, the photocatalytic activity can be remarkably enhanced [11] and used in applications such as: water purification, solar cells, removal of different pollutants and of different gases [12].

Further on, when adding  $\text{TiO}_2$  in polymer electrolytes, strengthened ionic conductivity and better mechanical properties are obtained [13]. Also an important feature of  $\text{TiO}_2$  particles is represented by the light scattering property. This property vary with the shape, size, concentration, surface roughness and spatial arrangement of the particles, and is important for industrial applications such as paint industry and solar cells [14].

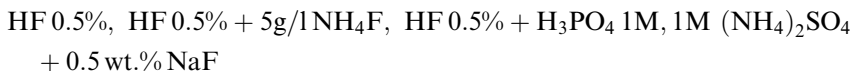
Regarding elaboration of controllable properties of oxide layers on Ti surface, anodizing seems to be promising nano-modification technique [15,16] and, in this light, has been found set of Ti anodizing conditions which create nanotubes with mimetic features of natural bone [16]. Taking into account that collagen, the main organic component of bone, is a triple helix 300 nm in length, 0.5 nm in width, and hydroxyapatite (HA), the inorganic component has particle sizes around 20–40 nm long it is possible to assume that bone cells are accustomed to a nanoscale tubular environment rather than the micron-scale environment [17]. Moreover, biocompatibility studies indicated bone forming functionality on diameter controlled  $\text{TiO}_2$  nanotube surfaces [18] and how  $\text{TiO}_2$  diameter directs cell fate as an expression of relation between nanosize and vitality [19].

## Experimental

### *Materials and Methods*

Ti samples were 99.76% purity, donated by Institute for Non-Ferrous and Rare Metals, Bucharest. The other components were, Fe, Al,  $\text{O}_2$ ,  $\text{N}_2$ , C. The samples are foils with 2 mm thickness and were prepared being mechanically polished, degreased in acetone, washed for five minutes in de-ionized water and then immersed in a HF and  $\text{HNO}_3$  solution for 30 seconds. Then washed again with de-ionized water for five minutes and dried at 40°C. Samples were mounted like an anodic electrode in a electrochemical cell with a two-electrode configuration, serving as cathode a Pt grid. A constant voltage between anode and cathode was applied by a power supply and current transients were recorded. The anodizing procedure

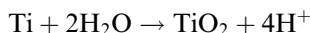
was performed at room temperature for 120 minutes at 20 V constant value in a mixture of fluoride as following:



Surface analysis have been investigated by scanning electron microscopy (SEM), atomic force microscopy (AFM), and contact angle measurements for various anodizing conditions. The surfaces changes in the topography and nanotubes diameter as a function of anodizing electrolyte were observed using Environmental Scanning Electron Microscope FEI/Phillips XL30 ESEM, with pressure 0.7 Torr. Pores diameter was calculated with Image J program. The morphological modifications analysis was completed with roughness evaluation carried out with an atomic force microscope from APE Research, Italia. The balance hydrophilic/hydrophobic was evaluated from contact angle measurements, using a Contact Angle Meter – KSV Instruments CAM 100. The surface hydrophilicity of anodizing Ti was studied by measuring static contact angle with sessile drop of distilled water deposited on the sample surface as a function of electrolyte composition. Each contact angle value is the average of minimum 10 measurements. The investigation was carried out with an accuracy of  $\pm 1^\circ$  at a temperature of 25°C. Electrochemical methodology for stability involved open circuit potential determinations in Na Cl and the cyclic potentiodynamic polarization measurements applied beginning from  $-0.8 \text{ V}$  to  $+4.0 \text{ V}$  (vs. SCE). Cyclic polarization was performed with a scan rate of  $2 \text{ mV/sec}$ , using a Voltalab 40 equipment with its Volta Master 4 program. Also, the linear polarization measurements were carried out with the purpose to obtain the polarisation resistance ( $R_p$ ), the corrosion current densities ( $i_{\text{corr}}$ ) and the corrosion rates ( $V_{\text{corr}}$ ). A Voltalab 80 equipment with its VoltaMaster 4 program were used and as testing solution was chosen Hank bioliquid with the following composition; NaCl 8 g/l; CaCl<sub>2</sub> 0.14 g/L; KCl 0.4 g/L; MgCl<sub>2</sub>·6H<sub>2</sub>O 0.1 g/L Na<sub>2</sub>HPO<sub>4</sub>·12H<sub>2</sub>O 0.06 g/L; MgSO<sub>4</sub>·7H<sub>2</sub>O 0.06 g/lL glucose 1 g/L.

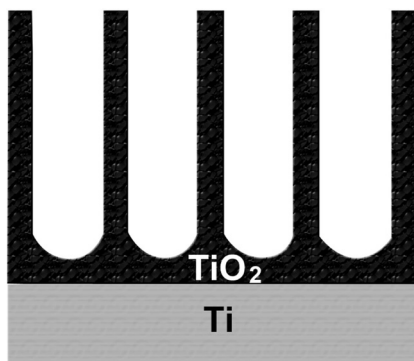
## Results and Discussion

In the majority of anodizing electrolytes for Ti, a compact TiO<sub>2</sub> structure is obtained, according to following reaction:



The oxide is amorphous if the anodizing took place at 20 V, or crystalline at higher voltage. Generally depending on conditions, a mixture of crystalline anatase and rutile is formed. In fluoride-containing electrolytes, an oxide layer forms on the surface of titanium as well at the beginning. Depending on the conditions, after a time, in the presence of F<sup>−</sup> the oxide layer partially dissolves and forms pits according to the reaction  $\text{TiO}_2 + 6\text{HF} \rightarrow [\text{TiF}_6]^{2-} + 2\text{H}_2\text{O} + 2\text{H}^+$ .

These concurrent processes anodic oxidation and dissolution leads to the formation of nanotube arrays, corresponding to a schematic proposed model (Fig. 1) according to literature data [7–10], including our previous work with elemental surface analysis [10].



**Figure 1.** Schematic model of nanotubes formation.

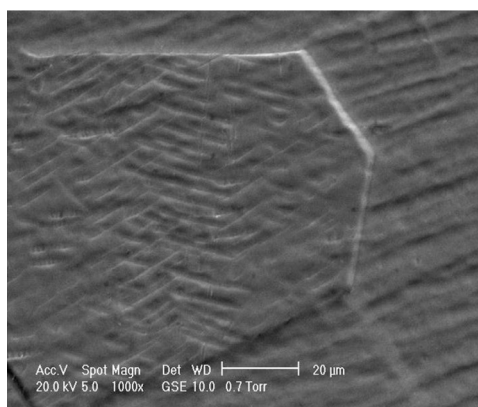
In the case of electrolytes with fluoride on  $\text{TiO}_2$  compact structure, self – organized  $\text{TiO}_2$  nanotubes are grown as a result of monitoring conditions as potential, time and temperature.

*Surface analysis.* The surface SEM images are presented in Figure 2, where a top view of  $\text{TiO}_2$  nanotubes fabricated in HF 0.5% is together with a microscopic image of a native  $\text{TiO}_2$  microstructure.

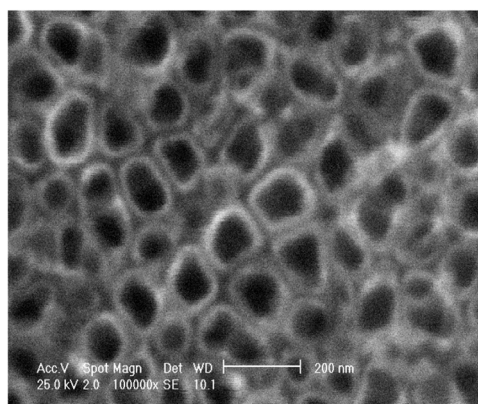
The 2D AFM images of  $\text{TiO}_2$  self-organized layers elaborated in various fluoride solutions are presented in Figure 3, which permitted the evaluation of roughness as Root Mean Square (RMS) parameter  $R_q$ , and the Roughness Average ( $R_a$ ).

The roughness values obtained for nanotubes are listed in Table 1 and compared with 11 and 15 nm respectively values for reference specimen, the natural passivated titanium surface [10]. In Table 1, together with roughness values, the diameters and contact angle are presented as function of anodizing conditions.

In a previous work [20] the nanostructure fabrication was pursued using glycerol containing 4% water and 0.36 M  $\text{NH}_4\text{F}$ . Starting at 20 V anodizing procedure gives self organized nanotubes with 40–55 nm diameter and clear an ordered aspect, but with the increase in voltage, the ordered structures shift from nanotubular aspect towards a porous distribution. At 40 V, the nanotubes are incorporated by porous structures of the same diameter. The incorporation process accentuates for the higher voltage and at 80 V applied voltage gives a final porous-only surface. Such data sustain the idea of a strong dependence between  $\text{TiO}_2$  nano pattern and fabrication conditions. The contact angle values for native  $\text{TiO}_2$  is 49 and this is a reference value. The contact angle values for anodizing Ti as function of electrolyte composition and nanotube geometry varied from a very weak hydrophilic value (83) to the best hydrophilic value as 16. Such results indicate that obtaining nanotubes architecture is not always a way to increase hydrophilicity of surfaces. Taking into account that wettability is a crucial factor in cell adhesion, self cleaning, etc., such variation for hydrophilic/hydrophobic balance supports the idea that for each potential application nanostructure could be an improvement only for a specific geometry. Referring to biomedical application, to cell adhesion in particular as an aspect of biocompatibility literature data affirm that osteoblast adhesion is enhanced on Ti anodized to possess nanotubes compared to those not anodized [17] and this fact should be correlated both to surface roughness and to contact angle, parameters that for native  $\text{TiO}_2$  are usually direct correlated, for smoother surfaces the contact angle being larger



(a)



(b)

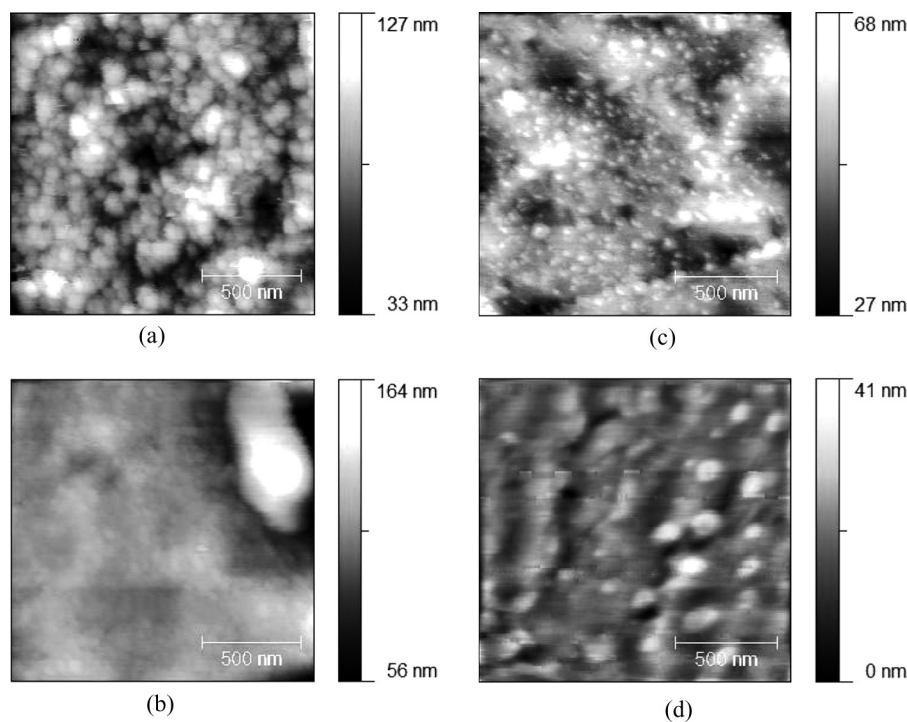
**Figure 2.** SEM structure of the (a)  $\text{TiO}_2$  native passive stratum, (b)  $\text{TiO}_2$  nanotubes self-organized layer.

[21]. That means that smooth surface can improve cell adhesion, but this fact is more complex in nanotubes cases where  $\text{TiO}_2$  diameter seems to direct cell fate [19,22].

*Electrochemical Stability.* The initial event during the immersion of titania nanotubes in bioliquids, is the hydrolysis and the establishing of the equilibrium surface-solution. This dissolution process may conduct to species as  $\text{Ti}(\text{OH})_2$  or hydroxocomplex like  $\text{TiO}(\text{OH})_2$ . Immediately after immersion in bioliquids as NaCl 0.9% as can be seen in Figure 3, the corrosion potential presents electronegative values. A tendency to more noble values are taking place after a short period of behavior in NaCl, the difference consisting in the range of potential values, which is in the more electropositive domains for the self organized nanotubes structures.

According to Figure 4, dissolution and repassivation of Ti are expressions of the film stability in both cases, but both aspects are more pronounced in the case of native  $\text{TiO}_2$ . The tendency to steady state is evident for  $\text{TiO}_2$  nanotubes after shorter period of time.

Regarding cyclic voltammetry recorded in Hank biofluids, the curves for various nanotubes architectures presented in Figure 5 indicate as a more stable  $\text{TiO}_2$  geometry, the one elaborated in HF 0,5% + 5 g/l  $\text{NH}_4\text{F}$ .



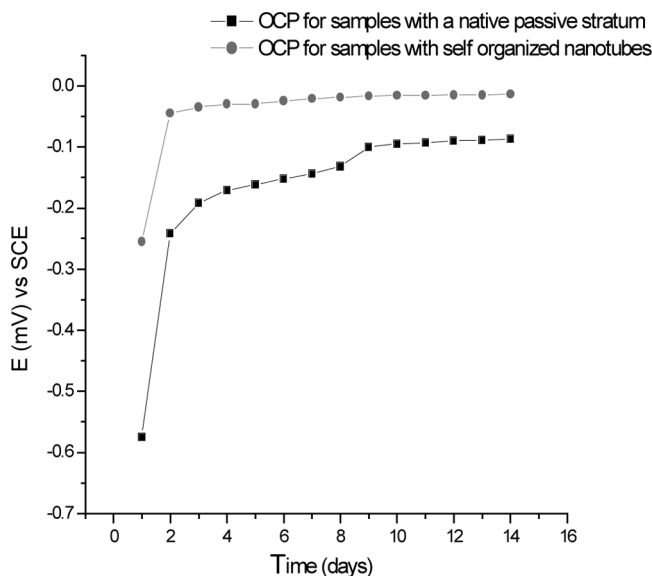
**Figure 3.** Image of Ti surface anodized in: (a) HF 0.5%, (b) HF 0.5% + 5 g/l  $\text{NH}_4\text{F}$ , (c) HF 0.5% +  $\text{H}_3\text{PO}_4$  1 M, (d) 1 M  $(\text{NH}_4)_2\text{SO}_4$  + 0.5 wt.% NaF.

Electrochemical parameters from Tafel plots are subject of Table 2. Comparing the obtaining values can be observed that the corrosion potential for Ti/ $\text{TiO}_2$  nanotube electrode are anodical shifted from  $-162,4\text{ mV}$  to  $-62,2\text{ mV}$  by changing the anodizing condition and as a consequence the nanotubes geometry. Also, it is clear from the calculated values that  $\text{TiO}_2$  nanotube coatings increase the surface stability by reducing the corrosion current densities and increase the polarization resistance in a specific manner as a function of their dimensions.

According to Table 2 all corrosion rates for various  $\text{TiO}_2$  nanotubes fabricated in different electrolytes correspond to the class “very stable.” The smallest corrosion rate from table 2 which sustained the best stability for nanotubes fabricated in the mixture HF 0.5% + 5 g/l  $\text{NH}_4\text{F}$  is associated with the largest passive domain from Figure 4 and with the smallest diameter. Taking into account corrosion rate for

**Table 1.** Surface characteristics as a function of anodizing electrolyte composition

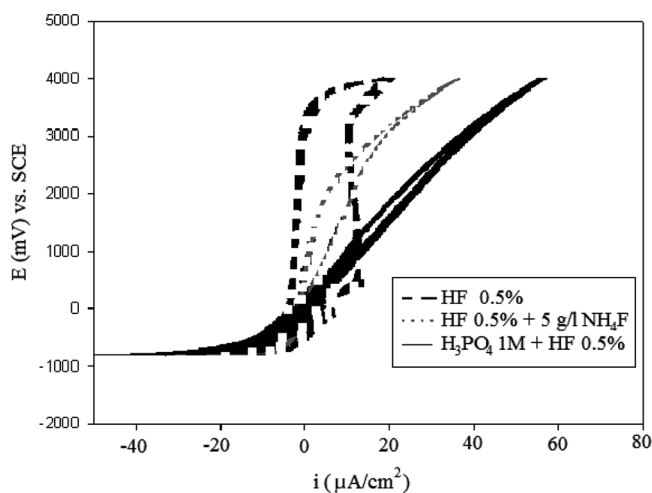
No.	Electrolyte composition	$R_a$ (nm)	D Diameter (nm)	$R_q$ (RMS) (nm)	Contact angle, °
1	H HF 0.5%	19	100	23	83,39
2	H HF 0.5% + 5 g/l $\text{NH}_4\text{F}$	16	60	21	55,45
3	H HF 0.5% + $\text{H}_3\text{PO}_4$ 1 M	14	400	19	77,45
4	1 $(\text{NH}_4)_2\text{SO}_4$ + 0.5 wt.% NaF	23	120	29	16



**Figure 4.** The evolution of potential in time for  $\text{TiO}_2$  nanotubes (fabricated in  $(\text{NH}_4)_2\text{SO}_4 + 0.5 \text{ wt.}\% \text{ NaF}$ ) and for native  $\text{TiO}_2$ .

natural passive stratum which is  $68,28 \text{ } (\mu\text{m}/\text{year})$ , such data reveal nanotubes as more stable structure.

The stability test of nanotubes  $\text{TiO}_2$  structure in Hank solution indicated that the corrosion current densities obtained by Tafel lines extrapolation decrease in the following direction:  $i_{\text{corr}} \text{ HF } 0.5\% + \text{H}_3\text{PO}_4 \text{ 1 M} > i_{\text{corr}} \text{ HF } 0.5\% > i_{\text{corr}} \text{ HF } 0.5\% + 5 \text{ g/l NH}_4\text{F}$ . The same range is for the decrease of nanotubes diameter. The increase of electrochemical stability in other biofluids as saliva was related in a previous study [23] to an increase of biocompatibility. The behavior of fibroblast



**Figure 5.** Cyclic voltammetry curves for nanotubes fabricated in various electrolytes.



**Table 2.** Electrochemical parameters from Tafel plots

Anodizing on conditions	Diameter, (nm)	$E_{\text{cor}}$ (mV) vs. SCE	$I_{\text{cor}}$ ( $\mu\text{A}/\text{cm}^2$ )	$V_{\text{cor}}$ ( $\mu\text{m}/\text{y}$ )	$R_p$ ( $\Omega\text{cm}^2$ )
HF 0.5%	100	−89,6	2.31	6.49	1359.3
HF5% + 5 g/l $\text{NH}_4\text{F}$	60	−62,4	1.97	2.98	709.14
H 0.5%HF + $\text{H}_3\text{PO}_4$ 1 M	400	−162,4	9.98	8.85	2495.6

cells was evaluated in the immunofluorescent signals which revealed a better fibronectin expression and fine reticular organization on  $\text{TiO}_2$  nanotubes compared to the native  $\text{TiO}_2$ . This suggests a more tight cell adhesion on such support, the cell density being higher in this case. It is an indication that nanotubes are preferred by the cells. Recent papers have found that osteoblast adhesion is enhanced on Ti anodized to possess nanotubes [17] compared to those anodized to possess nanoparticles and those not anodized at all, and mesenchymal stem cells has size selective behavior.

## Conclusions

1. Using anodic deposition with an applied voltage of 20 V for 2 hours at room temperature in a mixture of various fluoride electrolytes, different architecture of highly ordered self organized  $\text{TiO}_2$  nanotubes layers were obtained.
2. The surface was analysed with scanning electron microscopy and atomic force microscopy and revealed a porous nanotube structure of the oxide surfaces with an average diameter between 60 and 400 nm, and a somewhat rough surface, depending on the electrolyte content.
3. The contact angle data indicated a hydrophilic domain for all studied nanostructure, but depending of their fabrication condition the hydrophilic character varied from very weak (83.39) to strong (16).
4. The stability test of nanotubes  $\text{TiO}_2$  structure in Hank solution indicated that the corrosion current densities obtained by Tafel lines extrapolation decrease in the following direction:  $i_{\text{corr}}$  HF 0.5% +  $\text{H}_3\text{PO}_4$  1 M >  $i_{\text{corr}}$  HF 0.5% >  $i_{\text{corr}}$  HF 0.5% + 5 g/l  $\text{NH}_4\text{F}$ . The same range was put in evidence for the decrease of nanotubes diameter.
5. The various geometry and hydrophilic character of self-organized  $\text{TiO}_2$  nanotubes layers induced different characteristics which can be exploit in different potential applications, from biomedical to environment and energy.

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